Original Article Gender differences in degenerative Iumbar scoliosis spine flexibilities

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Abstract: Objectives: The incidence of adolescent idiopathic scoliosis is higher in girls, but spine deformities are more severe in boys. We aimed to identify gender differences of mechanical factors involved in adult degenerative scoliosis (DS). Methods: 20 male (60.35 ± 6.77 years) and 19 female (58.89 ± 9.15 years) specimens of cadaveric lumbar spines were divided into 3 groups comprised of a Cobb angle >10° (DS), a Cobb angle <10° but >3° (predegenerative scoliosis (PS)) and intervertebral disc angles <3° in which the Cobb angle could not be measured (non-degenerative scoliosis (NS)), respectively. Spine data were collected for flexion/extension (FE), lateral bending (LB), axial torsion (AT), range of motion (ROM), neutral zone (NZ) and the neutral zone ratio (NZR). Results: There was no significant difference regarding the severity of DS between male and female specimens. Only in males were ROM_{AT} (P=0.001), NZ_{AT} (P<0.001), NZ_{FE} (P=0.045), NZ_{LB} (P=0.002) as well as NZR_{AT} (P<0.001) and NZR_{LB} (P=0.001) values significantly lower in right compared to left scoliosis. With the exception of ROM_{AT} in DS specimens, ROM_{AT}, NZ_{FE} and ROM_{LB} values were significantly higher in females than those in males for the DS, PS and NS specimens. NZ_{AT}, NZ_{FE} and NZ_{LB} values were significantly higher in PS and NS female specimens. NZR_{AT} was significantly lower in female Scoliosis specimens, the rigidness of spines was higher in males than in females and more pronounced in right than in left scoliosis, but only in males.

Keywords: Biomechanics, degenerative scoliosis, initial scoliosis nature, occurrence, development

Introduction

Scoliosis in adults is a common term including any form of scoliosis in mature individuals regardless of whether the deformity begins before or after skeletal maturity [1]. Common forms comprise adult idiopathic scoliosis (AdIS) and de novo adult degenerative scoliosis (ADS); the former occurs as a continuation of adolescent idiopathic scoliosis and the latter is caused by progressive degenerative changes [2].

Degenerative scoliosis (DS) is the constitutional alignment of the spinal column caused by degeneration of the intervertebral discs and facet joints after skeletal maturation in which the coronal Cobb angle is greater than 10° [3-5]. As the lumbar and thoracolumbar spinal segments are usually affected [6], it can also be called degenerative lumbar scoliosis (DLS). Xu and colleagues [7] reported that the prevalence of DS in a Chinese Han population of individuals over 40 years of age was approximately 13.3% and it increased with age. The basic pathophysiology of DS remains unclear, but most scholars believe that the pathological basis is asymmetric intervertebral disc and facet joint degeneration, leading to vertebral tilt and abnormal activities, resulting in spinal instability and asymmetry as well as the formation of three-dimensional spinal deformities [8]. Studies conducted by Murata and colleagues [9] reported that lumbar disc degeneration in any segment was likely to be a trigger for degenerative lumbar scoliosis. Present studies have considered age [10], gender [7], race [11], osteoporosis [12], lumbar lateral listhesis [13], relationship of L5 to the intercrest line [14] rotatory deformity and lateral spondylolisthesis of the L3 vertebra [15, 16] as well as a smaller L4



Figure 1. Scheme for the diagnosis of the severity of scoliosis. A. Measurement of wedge angle in the intervertebral space; B. Measurement of the Cobb angle in a case where the intervertebral disc angle was $>3^{\circ}$.

size and L4 tilt at baseline [10] to be potential factors that lead to the progressive increase of scoliosis. Various studies have reported that the incidence of adolescent idiopathic scoliosis was higher in girls than in boys, though its severity was greater in boys [17-22]. However, less information has been published on gender differences of DS and therefore in the present study gender differences of spine range of motion (ROM) and neutral zone (NZ) values in specimens with DS were evaluated.

Materials and methods

The present research was carried out in the Spine and Biomechanics Laboratory, Department of Neurosurgery, Allegheny Health Network in the USA. Since the cadaveric investigations did not involve human subjects, institutional review board approval for research presented in this article was not necessary. Thirtynine frozen human lumbar spine specimens of 20 males and 19 females from T12 to S1 were obtained following institutional approval of the Department of Neurosurgery of the Allegheny Health Network.

The fresh cadaveric whole lumbar spines from T12 to S1 specimens were sealed in double plastic bags and frozen at -20°C until required for analysis. Before testing, the specimens were thawed for 24 h at room temperature. The musculature and soft tissue were removed from each specimen but sparing the osteoligamentous structures. Each specimen was fixed onto 2 potting rings at T12 and the sacrum, making sure the rings and specimen were aligned. A total of 195 functional spinal units (FSU) were tested (from L1 to S1). All specimens were scanned by computed tomography (CT) at a 0.6 mm resolution and the images imported into ScanIP (version 6.0, Simpleware, Exeter, UK) in order to create 3-D models of the vertebral bodies. The intervertebral disc angles (angle between the tangential lines of the inferior endplate of a vertebra and the superior endplate of the next vertebra) (Figure 1A) were measured. If the intervertebral disc angle was

	Male (n=20)	Female (n=19)	P-value
Age (years), mean ± SD	60.35±6.77	58.89±9.15	0.574
Different scoliosis, n (%)			0.999
NS	12 (60.0)	13 (68.4)	
PS	5 (25.0)	4 (21.1)	
DS	3 (15.0)	2 (10.5)	
FSU, n			0.497
NS	58	61	
PS	24	19	
DS	15	10	
Scoliosis orientation, n (%)			0.580
Left	6 (75.0)	3 (50.0)	
Right	2 (25.0)	3 (50.0)	
Scoliosis apex, n (%)			0.180
L1-2	0 (0.0)	1 (16.7)	
L2-3	3 (37.5)	0 (0.0)	
L3-4	1 (12.5)	3 (50.0)	
L4-5	4 (50.0)	2 (33.3)	
		c	

 Table 1. Basic characteristics

Abbreviations: DS, degenerative scoliosis; FSU, functional spinal unit; NS, non-degenerative scoliosis; PS, pre-degenerative scoliosis.

more than 3°, the lumbar spine Cobb angle was measured from the upper-level vertebra to the lower-level vertebra (**Figure 1B**). In cases where the intervertebral disc angles were $<3^{\circ}$ the spines were considered to comprise nondegenerative scoliosis (NS). If the intervertebral disc angles were $>3^{\circ}$ and the Cobb angles $<10^{\circ}$ but $>3^{\circ}$ the spines were considered to represent pre-degenerative scoliosis (PS) whereas a Cobb angle $>10^{\circ}$ indicated DS.

Kinematic measurements

The locations and orientations of the vertebrae were monitored using a motion capture system (Optotrak, Northern Digital Instruments, Waterloo, ON, Canada). Kinematic data were obtained for flexion extension (FE), lateral bending (LB) and axial torsion (AT) using a 6-degree-offreedom spine tester (Bose, Smart Test Series, Eden Prairie, MN, USA), with 3 cycles of sinusoidal loading (max \pm 7.5 N, 0.005 Hz); data from the 3rd cycle were used for analyses.

Euler angles were calculated from each vertebral tracking body to its inferior neighbor in the sequence Xy'z". The FE ROM, LB ROM and AT ROM were defined as the ranges of the first Euler angle (α , corresponding to the X axis), the second Euler angle (β , corresponding to the y' axis) and the third Euler angle (y, corresponding to the z axis). The NZ was a measure of residual vertebral motion from the neutral position at the beginning of the third load cycle under zero load. The neutral zone ratio (NZR) was the quotient of NZ and ROM.

Statistical analysis

All statistical analysis was conducted using SPSS (Version 22, IBM, Armonk, New York, USA). The differences of ROM, NZ and NZR between different scoliosis orientation and scoliosis angle sizes were analyzed using one-way ANOVA with a post hoc Bonferroni correction. The differences of ROM and NZ between different scoliosis positions are represented by curves. Statistically significant differences were defined as a *P*-value <0.05.

Results

The specimens were obtained from 3 Negroid and 36 Caucasian individuals whose ages were 60.35 ± 6.77 years for males (n=20) and 58.89 ± 9.15 years for females (n=19). There were no significant gender differences regarding scoliosis grading and FSU numbers as well as for the orientation and scoliosis apex locations (**Table 1**).

Biomechanical effect of scoliosis orientation on scoliosis

In the DS and PS groups combined, 9 specimens had left orientation scoliosis and 5 right orientation scoliosis. There were 187 FSUs from which the ROM data were derived and 186 FSUs from which the NZ and NZR data were derived.

There was no difference in ROM data between left and right scoliosis orientation in females, but in males the range of motion-axial torsion (ROM_{AT}) was significantly lower in right scoliosis (*P*<0.001). Otherwise, the ROM_{AT}, range of motion-flexion extension (ROM_{FE}) and the range of motion-lateral bending (ROM_{LB}) values were all significantly higher in females than in males (ROM_{FE}: P_{Left} =0.001, P_{Right} =0.005; ROM_{LB}: P_{Left} <0.001, P_{Right} =0.001). Similarly, neutral zoneaxial torsion (NZ_{AT}), neutral zone-flexion extension (NZ_{FE}) and neutral zone-lateral bending (NZ_{LB}) values in right scoliosis were significantly higher in females than in males (*P*=0.005, *P*=0.006, *P*<0.001, respectively), an apparent trend also visible for left scoliosis but without statistical significance. In males, all NZ_{AT}, NZ_{FE} and NZ_{LB} values were significantly lower in right scoliosis compared to left scoliosis (*P*<0.001, *P*=0.045, *P*=0.002, respectively). NZ_{AT}, neutral zone ratio-axial torsion (NZR_{AT}) and neutral zone ratio-lateral bending (NZR_{LB}) values were similar in left scoliosis of both genders, but lower in males than in females. NZ_{AT} and NZR_{LB} were significantly lower in right than in left scoliosis only for males (both *P*<0.001) (**Table 2**).

Biomechanical effect of the scoliosis angle on scoliosis

With the exception of ROM_{AT} in DS specimens, all other ROM_{AT}, ROM_{FE} and ROM_{LB} values were significantly higher in females than in males for all DS, PS and NS specimens (ROM_{AT}: P_{PS} <0.001, $P_{\rm NS}$ =0.002; ROM_{FE}: $P_{\rm DS}$ =0.019, $P_{\rm PS}$ <0.001, $P_{\rm NS}$ <0.001; ROM_{LB}: $P_{\rm DS}$ =0.005, $P_{\rm PS}$ <0.001, $P_{\rm NS}$ <0.001). ROM_{AT} differed significantly between the 3 groups in female and male specimens (P=0.012, P=0.002, respectively), but ROM_{IB} values were only significantly different between the groups for females (P=0.012). NZ_{AT}, NZ_{FE} and NZ_{LB} values were significantly higher in females in the PS and NS specimens (all P<0.05), but only NZ_{LB} was significantly different within the female groups (P=0.008), whereas only NZ_{AT} differed significantly within the male groups (P<0.001). NZR_{AT} was significantly lower in the female DS samples, which was due to similar ROM_{AT} but higher NZ_{AT} values of male specimens. For PS specimens, significantly greater ROM _{AT} values in combination with significantly greater NZ $_{\rm AT}$ data led to a significantly higher NZRAT value in females (both P=0.031). With the exception of NZR_{FF} in male specimens all other NZR_{AT}, neutral zone-flexion extension (NZR_{FE}) and NZR_{LB} values were different in the 3 groups (all P<0.05) (Table 3).

Biomechanical effects of scoliosis apex positions on spine flexibilities

The scoliotic spine had the least ROM_{AT} when its apex was located at the L2-3 level and exhibited the largest ROM_{FE} and ROM_{LB} values when its apex was located at the L3-4 level. The apex level, however, did not have the largest ROM of the entire spine (**Figure 2A-C**). The scoliotic spine had the least NZ_{AT} when its apex was located at the L2-3 level and had the largest NZ_{FE} and NZ_{LB} when its apex was located at the L3-4 level (**Figure 2D-F**).

Taken together, the results showed that the spine ROM in men with DS was worse than that in women. Especially degenerated right spinal curvatures due to the DS were more rigid in men and the difficulty of orthopedic surgery may be greater in males than in females.

Discussion

To evaluate the factors that affect the occurrence and development of DS, researchers have performed imaging studies through clinical follow-ups [7, 10, 16, 23], but biomechanical research literature has rarely been published. Unlike adolescent idiopathic scoliosis, DS has mild coronal Cobb angles, mostly within 10-20° [8, 24]. In the present study, we carried out biomechanical tests on NS, PS and mild to moderate DS with Cobb angles <15° to determine the biomechanical characteristics. The total ROM of a spinal segment is commonly divided into neutral and elastic zones. For spinal stability the NZ must be stabilized and motions occurring within the NZ must be controlled in order to maintain the size of the neutral zone. Instability of the spine develops when the NZ increases relative to the ROM, which is expressed by the NZR formula [25, 26]. In a recent study on whole trunk NZ quantification of scoliotic lumbar spines, especially the axial twist, NZ was significantly greater in scoliosis specimens [27], which was reflected in significantly higher NZ_{AT} and NZR_{AT} values of male compared to female DS specimens in the present study. Otherwise, ROM values were generally higher in females than those in males, but this was accompanied by usually higher NZ values, leading to more similar NZR values between genders. In particular, ROM_{FF} values were significantly lower in male than those in female NS, PS and DS specimens, indicating generally higher stiffness in males [28].

Different findings were found during the clinical follow-up process regarding the role of scoliosis orientation in the development of DS. Some scholars believe that the initial orientation of scoliosis is not correlated with the progression of scoliosis [15], while Chin and colleagues [29]

Gender difference in degenerative lumbar scoliosis spine rigidness

		ROM	ROM _{AT}	ROM	ROM	NZ	NZ _{AT}	NZ _{FE}	NZ	NZR	NZR _{AT}	NZR _{FE}	NZR
Left scoliosis	Female	FSU, n=15	6.33±1.98	12.30±3.62	11.12±1.94	FSU, n=14	1.43±1.02	3.48±2.36	3.07±2.56	FSU, n=14	0.21±0.09	0.28±0.15	0.26±0.18
	Male	FSU, n=29	4.71±2.99	8.38±3.20	7.93±2.33	FSU, n=29	1.17±0.91	2.25±1.97	1.77±1.41	FSU, n=29	0.23±0.12	0.22±0.15	0.22±0.12
	P-value	-	0.066	0.001	<0.001	-	0.396	0.079	0.092	-	0.527	0.209	0.431
Right scoliosis	Female	FSU, n=14	5.44±2.29	11.36±3.30	11.70±3.01	FSU, n=14	1.08±0.92	2.57±1.09	2.17±0.92	FSU, n=14	0.18±0.10	0.23±0.07	0.19±0.06
	Male	FSU, n=10	2.46±1.05	7.71±2.06	7.42±2.53	FSU, n=10	0.24±0.20	1.34±0.79	0.83±0.33	FSU, n=10	0.09±0.04	0.17±0.07	0.12±0.05
P-value (Left vs Right)	P-value	-	<0.001	0.005	0.001	-	0.005	0.006	<0.001	-	0.006	0.064	0.011
	Female	-	0.272	0.473	0.542	-	0.351	0.204	0.230	-	0.454	0.221	0.158
	Male	-	0.001	0.541	0.556	-	< 0.001	0.045	0.002	-	<0.001	0.168	0.001

 Table 2. Comparison of ROM, NZ and NZR between different scoliosis orientations

Note: Overall differences were compared using ANOVA. Abbreviations: NZ, neutral zone; NZ_{at}, neutral zone-axial torsion; NZ_{FE}, neutral zone-flexion extension; NZ_{LE}, neutral zone-lateral bending; NZR, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone; NZ_{at}, neutral zone, flexion; NZR_e, neutral zone-flexion extension; NZR_t, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_t, neutra

Table 3. Comparison of ROM, NZ and NZR between different scoliosis groups

		ROM	ROM _{AT}	ROM _{FE}	ROM	NZ	NZ _{AT}	NZ _{FE}	NZ	NZR	NZR _{AT}	NZR _{FE}	NZR
NS	Female	FSU, n=61	4.31±2.58	10.64±3.71	9.50±2.88	FSU, n=61	0.85±1.11	2.39±1.91	1.77±1.09	FSU, n=61	0.15±0.08	0.20±0.10	0.18±0.09
	Male	FSU, n=58	3.10±1.34	8.19±3.01	7.47±2.24	FSU, n=58	0.46±0.36	1.68±1.07	1.14±0.53	FSU, n=58	0.13±0.06	0.19±0.07	0.15±0.05
	P-value	-	0.002	<0.001	<0.001	-	0.011	0.014	<0.001	-	0.155	0.522	0.029
PS	Female	FSU, n=19	6.24±2.36	11.9±3.57	11.42±2.2	FSU, n=18	1.48±1.09	3.40±2.13	2.96±2.27	FSU, n=18	0.21±0.10	0.29±0.13	0.25±0.16
	Male	FSU, n=24	3.48±1.84	8.03±2.94	7.49±2.62	FSU, n=24	0.66±0.72	1.96±1.61	1.52±1.29	FSU, n=24	0.15±0.09	0.22±0.11	0.19±0.11
DS	P-value	-	<0.001	<0.001	<0.001	-	0.006	0.017	0.023	-	0.031	0.076	0.146
	Female	FSU, n=10	5.27±1.58	11.73±3.37	11.36±3.07	FSU, n=10	0.86±0.55	2.35±1.03	2.00±0.94	FSU, n=10	0.16±0.07	0.20±0.06	0.17±0.05
	Male	FSU, n=15	5.18±3.72	8.48±3.02	8.30±1.85	FSU, n=15	1.36±0.98	2.11±2.07	1.54±1.32	FSU, n=15	0.26±0.13	0.19±0.17	0.20±0.11
Overall P-value in gender groups	P-value	-	0.932	0.019	0.005	-	0.156	0.713	0.354	-	0.031	0.871	0.389
	Female	-	0.012	0.343	0.012	-	0.091	0.126	0.008	-	0.031	0.010	0.025
	Male	-	0.002	0.903	0.443		<0.001	0.490	0.126	-	< 0.001	0.566	0.038

Note: Overall differences were compared using ANOVA. Abbreviations: DS, degenerative scoliosis; NS, non-degenerative scoliosis; NZ, neutral zone; NZ_{st}, neutral zone-axial torsion; NZ_{ret}, neutral zone-flexion extension; NZ_{ret}, neutral zone-flexion extension; NZ_{ret}, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone ratio; NZR_{at}, neutral zone ratio-axial torsion; NZR_{ret}, neutral zone-flexion extension; NZR_{ret}, neutral zone-flexion extension; NZR_{ret}, neutral zone ratio-axial torsion; NZR_{ret}, neutral zone ratio-axial torsion; NZR_{ret}, neutral zone ratio-axial torsion; NZR_{ret}, neutral zone-flexion extension; NZR_{ret}, neutral zone ratio-axial torsion; NZR_{ret}, neutral zone ratio-a



Figure 2. ROM_{AT} , $\text{ROM}_{FE'}$, ROM_{LB} , NZ_{AT} , NZ_{FE} and NZ_{LB} of different scoliosis apex positions of PS and DS specimens. A. ROM_{AT} of different scoliosis apex positions; B. ROM_{FE} of different scoliosis apex positions; C. ROM_{LB} of different scoliosis apex positions; D. NZ_{AT} of different scoliosis apex positions; E. NZ_{FE} of different scoliosis apex positions; F. NZ_{LB} of different scoliosis apex positions; P. NZ_{AT} neutral zone-lateral bending; ROM_{AT} , range of motion-axial torsion; ROM_{FE} , range of motion-flexion extension; ROM_{IB} , range of motion-lateral bending.

studied 24 patients with DS and found that DS with initial left lateral scoliosis would worsen 3° per year and initial right lateral scoliosis would worsen 1° per year. In the present study, NZR_{AT} and NZR_{LB} values in left scoliosis specimens were significantly higher in the left compared to right scoliosis orientation, but only in males.

The higher stiffness of male vs female scoliosis specimens and the more pronounced involvement of left scoliosis might be explained by the fact that the musculature is the major active compound for spinal stability, since the movements within and especially beyond the neutral zone are mainly controlled by skeletal muscles [25], which are usually stronger in males.

Several studies have found that the most common apex of DS was located at L3 or L4, while rotatory deformity and lateral spondylolisthesis of the L3 vertebra may be a prognostic factor for DS in the elderly [3, 24]. In contrast, another study reported that the majority of apexes were located at L2-3 [30].

In the present study, we found that the scoliosis with an apex located at L3-4 had the highest ROM_{FE} , ROM_{LB} , NZ_{FE} and NZ_{LB} values compared

to any other apex, which is consistent with the conclusion that L3-4 is the most common subluxation segment through radiological evaluation of DS [31] and supported by other studies in which DS mainly occurred at the interspaces between L3 and L4 or L4-S1 [32]. These results support the theory that a scoliosis apex, located especially at L3-4, will assert more influence on DS than an apex located at any other level. However, data from the present study suggests that scoliosis with an apex located at L2-3 had the lowest ROM and NZ values, which findings require further investigation. Another result was that the vertebral segment apex was not the one where the spine ROM/NZ was largest since it was expected that the scoliosis apex should normally be the most unstable segment in the entire spine.

There are some limitations in our study including the low number of specimens, especially the L1-2 and L2-3 apex, and that only Cobb angles of <15° were included.

Conclusions

Although scoliosis spines did not differ significantly between different genders regarding severity, in the male they were generally stiffer and there was a significantly greater stiffness in the right compared to left scoliosis orientation, but only in males.

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Disclosure of conflict of interest

None.

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References

[1] Kelly A, Younus A and Lekgwara P. Adult degenerative scoliosis-a literature review. Interdiscip Neurosurg 2020; 20: 100661.

- [2] York PJ and Kim HJ. Degenerative scoliosis. Curr Rev Musculoskelet Med 2017; 10: 547-558.
- [3] Ploumis A, Transfledt EE and Denis F. Degenerative lumbar scoliosis associated with spinal stenosis. Spine J 2007; 7: 428-436.
- [4] Glassman SD, Bridwell K, Dimar JR, Horton W, Berven S and Schwab F. The impact of positive sagittal balance in adult spinal deformity. Spine (Phila Pa 1976) 2005; 30: 2024-2029.
- [5] Gupta MC. Degenerative scoliosis. Options for surgical management. Orthop Clin North Am 2003; 34: 269-279.
- [6] Aebi M. The adult scoliosis. Eur Spine J 2005; 14: 925-948.
- [7] Xu L, Sun X, Huang S, Zhu Z, Qiao J, Zhu F, Mao S, Ding Y and Qiu Y. Degenerative lumbar scoliosis in Chinese Han population: prevalence and relationship to age, gender, bone mineral density, and body mass index. Eur Spine J 2013; 22: 1326-1331.
- [8] Kobayashi T, Atsuta Y, Takemitsu M, Matsuno T and Takeda N. A prospective study of de novo scoliosis in a community based cohort. Spine (Phila Pa 1976) 2006; 31: 178-182.
- [9] Murata Y, Takahashi K, Hanaoka E, Utsumi T, Yamagata M and Moriya H. Changes in scoliotic curvature and lordotic angle during the early phase of degenerative lumbar scoliosis. Spine (Phila Pa 1976) 2002; 27: 2268-2273.
- [10] Jimbo S, Kobayashi T, Aono K, Atsuta Y and Matsuno T. Epidemiology of degenerative lumbar scoliosis: a community-based cohort study. Spine (Phila Pa 1976) 2012; 37: 1763-1770.
- [11] Kebaish KM, Neubauer PR, Voros GD, Khoshnevisan MA and Skolasky RL. Scoliosis in adults aged forty years and older: prevalence and relationship to age, race, and gender. Spine (Phila Pa 1976) 2011; 36: 731-736.
- [12] Tomé-Bermejo F, Piñera AR and Alvarez L. Osteoporosis and the management of spinal degenerative disease (II). Arch Bone Jt Surg 2017; 5: 363-374.
- [13] Kleimeyer J, Liu N, Hu S, Cheng I, Alamin T, Grottkau B, Kukreja S and Wood K. The relationship between lumbar lateral listhesis and radiculopathy in adult scoliosis. Spine (Phila Pa 1976) 2019; 44: 1003-1009.
- [14] Faraj S, Holewijn R, van Hooff M, De Kleuver M, Pellisé F and Haanstra T. De novo degenerative lumbar scoliosis: a systematic review of prognostic factors for curve progression. Eur Spine J 2016; 25: 2347-2358.
- [15] Seo JY, Ha KY, Hwang TH, Kim KW and Kim YH. Risk of progression of degenerative lumbar scoliosis. J Neurosurg Spine 2011; 15: 558-566.
- [16] Tsutsui S, Yoshimura N, Watanuki A, Yamada H, Nagata K, Ishimoto Y, Enyo Y and Yoshida M.

Risk factors and natural history of de novo degenerative lumbar scoliosis in a communitybased cohort: the miyama study. Spine Deform 2013; 1: 287-292.

- [17] Wang W, Zhu Z, Zhu F, Sun C, Wang Z, Sun X and Qiu Y. Different curve pattern and other radiographical characteristics in male and female patients with adolescent idiopathic scoliosis. Spine (Phila Pa 1976) 2012; 37: 1586-1592.
- [18] Luk KD, Lee CF, Cheung KM, Cheng JC, Ng BK, Lam TP, Mak KH, Yip PS and Fong DY. Clinical effectiveness of school screening for adolescent idiopathic scoliosis: a large populationbased retrospective cohort study. Spine (Phila Pa 1976) 2010; 35: 1607-1614.
- [19] Mahabadi E, Ghandehari H, Mahdavi S, Tari S, Sotoudeh A and Safdari F. Adolescent idiopathic scoliosis: males versus females. Shafa Orthopedic Journal 2015; 2: e901.
- [20] Raggio CL. Sexual dimorphism in adolescent idiopathic scoliosis. Orthop Clin North Am 2006; 37: 555-558.
- [21] Ueno M, Takaso M, Nakazawa T, Imura T, Saito W, Shintani R, Uchida K, Fukuda M, Takahashi K, Ohtori S, Kotani T and Minami S. A 5-year epidemiological study on the prevalence rate of idiopathic scoliosis in Tokyo: school screening of more than 250,000 children. J Orthop Sci 2011; 16: 1-6.
- [22] Weinstein SL, Dolan LA, Cheng JC, Danielsson A and Morcuende JA. Adolescent idiopathic scoliosis. Lancet 2008; 371: 1527-1537.
- [23] Kim H, Kim HS, Moon ES, Yoon CS, Chung TS, Song HT, Suh JS, Lee YH and Kim S. Scoliosis imaging: what radiologists should know. Radiographics 2010; 30: 1823-1842.
- [24] Watanuki A, Yamada H, Tsutsui S, En-yo Y, Yoshida M and Yoshimura N. Radiographic features and risk of curve progression of de-novo degenerative lumbar scoliosis in the elderly: a 15-year follow-up study in a community-based cohort. J Orthop Sci 2012; 17: 526-531.

- [25] Panjabi MM. The stabilizing system of the spine. Part II. Neutral zone and instability hypothesis. J Spinal Disord 1992; 5: 390-396; discussion 397.
- [26] Mimura M, Panjabi MM, Oxland TR, Crisco JJ, Yamamoto I and Vasavada A. Disc degeneration affects the multidirectional flexibility of the lumbar spine. Spine (Phila Pa 1976) 1994; 19: 1371-1380.
- [27] Voinier SD, Agnew MJ and Carmouche JJ. Passive stiffness characteristics and neutral zone quality of the scoliotic lumbar torso in the principle anatomical planes of motion. Clin Biomech (Bristol, Avon) 2020; 80: 105162.
- [28] Rustenburg CME, Kingma I, Holewijn RM, Faraj SSA, van der Veen A, Bisschop A, de Kleuver M and Emanuel KS. Biomechanical properties in motion of lumbar spines with degenerative scoliosis. J Biomech 2020; 102: 109495.
- [29] Chin KR, Furey C and Bohlman HH. Risk of progression in de novo low-magnitude degenerative lumbar curves: natural history and literature review. Am J Orthop (Belle Mead NJ) 2009; 38: 404-409.
- [30] Yang C, Yang M, Chen Y, Wei X, Ni H, Chen Z, Li J, Bai Y, Zhu X and Li M. Radiographic parameters in adult degenerative scoliosis and different parameters between sagittal balanced and imbalanced ADS patients. Medicine (Baltimore) 2015; 94: e1198.
- [31] Gardner RO, Torrie PA, Bertram W, Baker RP and Harding IJ. A radiological evaluation of lateral vertebral subluxation associated with spinal stenosis in the lumbar spine in degenerative scoliosis. Spine Deform 2013; 1: 365-370.
- [32] Saleem S, Aslam HM, Rehmani MA, Raees A, Alvi AA and Ashraf J. Lumbar disc degenerative disease: disc degeneration symptoms and magnetic resonance image findings. Asian Spine J 2013; 7: 322-334.