# Original Article A novel technique in open wedge high tibial osteotomy to preserve the tibial slope: a basic study on cadaver and reconstruction CT scanning

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Received January 2, 2016; Accepted March 22, 2016; Epub June 15, 2016; Published June 30, 2016

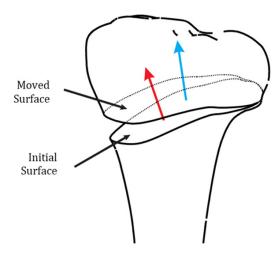
**Abstract:** High tibial osteotomy (HTO) is a well-established treatment option for uni-compartmental osteoarthritis. Recently, medial opening wedge HTO has become the primary surgical technique. It is very important in a high tibial open wedge osteotomy to keep the slope unchanged in the sagittal plane. The purpose of this study is to introduce a quantitative method of open wedge HTO to preserve the tibial slope without considering the osteotomy line. At first, mathematical calculations were concentrated, and the relations, formulas and tables were extracted. The results of formulas and tables were examined using software on reconstruction CT scanning of two intact tibiae (Level of Evidence: V). Then the results of the calculations were tested on five real cadavers. Software results showed that the changes in slope angle using the simplified formulas and tables are less than 0.5° in both subjects. Based on the *p*-value, the simplified formula or the tables can be used to correct the varus with minimal change in the slope and without considering osteotomy line. Results from osteotomies on 5 bones showed that changes in slope angle were significantly small. In 3 subjects, the change was less than 0.6°. Use of this new technique in open wedge HTO can result in good varus correction with minimal changes to the tibial slope, regardless of the orientation of the osteotomy line.

Keywords: High tibial osteotomy, open wedge, tibial slope, surgical technique, formula

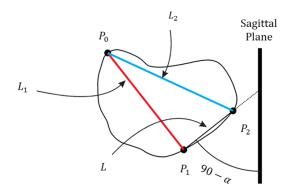
#### Introduction

High tibial osteotomy (HTO) is a well-established treatment option for uni-compartmental osteoarthritis associated with coronal deformity of the lower limb [1]. Clinical indications for an HTO include varus alignment of the knee associated with medial compartment arthritis, knee instability, medial compartment overload following meniscectomy, and osteochondral lesions requiring resurfacing procedures [1].

Many techniques have been described for HTO. The goal of the procedure is to realign the lower extremity and redistribute the joint forces applied to each compartment of the knee, thereby decreasing pain and improving overall function [1, 2]. The technique used for proximal tibia osteotomy has typically been the lateral closing wedge. In recent years, the medial opening wedge technique has gained popularity. The primary focus of both is to alter the weight-bearing axis in the coronal plane. Both methods have been shown to produce satisfactory clinical results in both the short- and longterm [1-4]. Lateral closing wedge HTO was once considered to be the standard of care: however. this technique is associated with fibular osteotomy or proximal tibiofibular joint disruption, peroneal nerve injury, more demanding subsequent total knee arthroplasty (TKA), and loss of bone stock [1]. Recently, medial opening wedge HTO has become the primary surgical technique [2]. Disadvantages associated with medial opening wedge HTO include the need for bone grafting and the risk of collapse or loss of correction [5].



**Figure 1.** The moved and initial surfaces with corresponding normal vectors (red vector corresponding to the initial surface and blue vector corresponding to the moved surface).



**Figure 2.** Presentation of defined points, lengths and angles on tibial cut plane. Sagittal Plane is the Sagittal Plane of whole body.

It is very important in a high tibial open wedge osteotomy to keep the slope unchanged in the sagittal plane; it should mimic the proximal tibial joint slope [6].

The proximal anteromedial cortex, when viewed in cross section, has an oblique or triangular shape, whereas the lateral tibial cortex is nearly perpendicular to the posterior margin of the tibia. Thus, in an open wedge high tibial osteotomy, if the wedge gap has an equal anterior and posterior diameter, the tibial slope will be increased [5].

Noyes et al. [7] showed that in order for the tibial slope to remain unchanged, the osteotomy line must be parallel to the tibial slope, and the most anterior gap of the osteotomy wedge at the tibial tubercle should be one-half the posteromedial gap. Every millimeter of gap error at the tibial tubercles results in approximately 2° of change in the tibial slope [7]. In some conditions, however, during the open wedge HTO, the osteotomy line may not be parallel to the tibial plateau. In such cases, it is necessary to find a method to keep the slope unchanged.

This study aimed to introduce a quantitative method of open wedge HTO to preserve the tibial slope without considering the osteotomy line. To the best of our knowledge, this is the first study to introduce a method for open wedge HTO that keeps the tibial slope unchanged despite the osteotomy line.

# Materials and methods

At first, calculations were concentrated, and then relations and tables were extracted from that data. In the next step, results from the previous part were tested in the 3D software. In the last step, the results of the calculation were tested on real cadavers, and the results were compared.

# Calculations

The first assumption is that the cut surface is a plane (smooth cut). Therefore, a plane equation can be written for the cut surface. Obviously, at least 3 points of the plane (non-aligned) were needed to make a unique plane. For convenience, we should be chosen so obtain coordinates of the 3 non-aligned points was a simple task. In this study, the three points were defined as follows:

• Point Zero: This point is the end of the cut, and when opening the osteotomy site, the bone fragments are driven around it. The coordinates of this point are (0,0,0).

• Point One: This point is on the cortical bone of the tibia; the surgeon can see it during surgery. An effort is made to select this point at the posterior medial cortex that is available to the surgeon. The coordinates of this point are  $(x_1, y_1, z_1)$ .

• Point Two: This point is similar to "Point One" on the same cortical tibia bone, the only differ-

Subject	Cutting Angle [Deg]	L <sub>1</sub> [mm]	L <sub>2</sub> [mm]	Correction Varus Angle [Deg]
#1 (parallel)	46	57.4	63.5	10
#1 (5° increase)	48	57.94	63.74	10
#2 (parallel)	46.41	59.7	61.34	10
#2 (10° increase)	46.41	47.74	51.22	10

**Table 1.** Subject parameters in the software in both

 parallel and non-parallel cut

Table 2. p-values for Figure 7's data, includeded 0 to 20 degree

Calculate From Table								
Parallel	Nonparallel							
1.51e-8	1.74e-6							
2.03e-8	1.06e-7							
	Parallel 1.51e-8							

ence being it is placed more on the frontal medial cortex. The coordinates of this point are  $(x_2, y_2, z_2)$  (**Figure 2**).

The two planes were defined as follows:

• Initial surface: Cropped area is located on the posterior piece of the tibia. It is assumed that the surface is fixed and does not move during surgery.

• Moved surface: After the cut, this surface is separated from the initial surface and displaced by rotating the inferior tibia fragment around Point Zero (**Figure 1**).

# Calculating the coordinates of points

Detecting the coordinates of two points on a complex surface like a tibia during surgery is a difficult task. Therefore, a simple method is proposed in this study that can obtain  $x_1$ ,  $x_2$ ,  $y_1$  and  $y_2$  coordinates.

Instead of calculating these four parameters, four new parameters are defined, the measurement of which is simpler for the surgeon than  $x_1, x_2, y_1$  and  $y_2$  coordinates. If the sizes of three sides of the triangle are known, a unique triangle can be produced on plan. To define the triangle direction, we can measure the angle between triangle height and sagittal plan (x axis). So:

- $L_1$  is the distance between points 1 and 0.
- $L_2$  is the distance between points 2 and 0.
- *L* is the distance between points 2 and 1.

•  $\alpha$  is the angle between triangle height and sagittal plan. If  $\swarrow \overline{P_1P_2}$  is the angle between x plan and line from 1 to 2 point:  $\alpha = 90 - \triangleleft \overline{P_1P_2}$  (Figure 2).

Height (z) on all three points is supposed to equal zero.

If *H* is the height of the triangle, and  $S_1$  and  $S_2$  are the distance of the point of impact of height with the rule of triangles to points

1 and 2, respectively, we have from the trigonometric relationships:

$$x_1 = H\cos\alpha + S_1\sin\alpha$$
 Eq. 1(a)

 $y_1 = Hsin\alpha - S_2 cos\alpha$  Eq. 1(b)

 $x_2 = H\cos\alpha - S_2\sin\alpha$  Eq. 1(c)

$$y_2 = H \sin \alpha + S_2 \cos \alpha$$
 Eq. 1(d)

Eq. 1 can also be proved:

S = S<sub>1</sub> = 
$$\frac{L_1^2 - L_2^2 + L^2}{2L}$$
 Eq. 2(a)

$$S_2 = \frac{-L_1^2 + L_2^2 + L^2}{2L}$$
 Eq. 2(b)

$$H = \frac{1}{2L} \sqrt{4L_1^2 L_2^2 - (L^2 - L_1^2 - L_2^2)^2}$$
 Eq. 2(c)

To obtain an accurate value of the opening of the mathematical techniques, solving the nonlinear system of 7 equations and 7 unknown variables is required. Due to the numerical solution, which is very complex, solving these 7 equations is almost impossible for the surgeon. To simplify the equations, several assumptions need to be applied, and the particular circumstances must be evaluated. It is assumed that coordinates x and y are any two points in two identical value and are different only in the value of z; it can be deduced from this assumption that the created triangle on the moved plan is the image of the triangle on the initial plan in the direction of z on the moved plan, and it is not rotated. Although the nature of the movement here has changed, because the angles are small, a good approximation can be made.

The slope angle cannot be changed. In this case the amount of sides opening can be extracted from this simple formula:

$$\begin{cases} W_1 = A.H - B.S \\ W_2 = W_1 + L.B \end{cases}$$
 Eq. 3

Where  $W_1$  and  $W_2$  are the openings of the wedges in points 1 and 2, respectively. *H* and S can be obtained from Eq. 2. Note that S was consid-

Table 3. Results from osteotomy on the tibia with new
way and without considering osteotomy orientation

- ,			0		
Subject			Cutting Angle	Chang of Slop Angle	Varus Angle Correction
			[Deg]	[Deg]	[Deg]
#1	60	65	45	0.55	7.76
#2	-	-	-	-	-
#3	65	70	45	0.39	10.05
#4	59	67	45	0.41	9.37
#5	63	66	45	1.87	7.09
	M	ean		0.8	8.57

ered equal to  $S_1$ . In **Figure 2**, *L* is the distance between points 1 and 2 and was considered equal to 25 mm in all surgeries. *A* and *B* could be determined from the following equation:

$A = \sin\alpha \tan\theta_{c}$	Eq. 4(a)
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 $B = \cos \alpha \tan \theta_{a}$  Eq. 4(b)

Where  $\theta c$  is the corrected angle of varus, which the surgeon is going to apply?

Because of the complex relationship between *H* and S, for the convenience of the surgeon, **Table 4** presents values of *H* and S in terms of  $L_1$  and  $L_2$  and for L = 25 mm. Note that the smaller parameter (usually  $L_1$ ) will be on the horizontal axis and the larger parameter (usually  $L_2$ ) on the vertical axis. For these two parameters, two values will be obtained, the first of which will be *H* and the second S.

Obtaining the two parameters A and B is also difficult for the surgeon. For simplicity, **Table 5** is presented that  $\alpha$  is the horizontal axis and  $\theta c$  is the vertical axis. As expected, obtaining the parameter  $\alpha$  in the tibia is difficult for the surgeon. Because the value of this angle is  $45^{\circ}\pm6^{\circ}$  (Noyes, Goebel, & West, 2005), the value of  $\alpha$  can be 45°.

It is recommended that when using the table, parameters measured ( $L_1$  and  $L_2$ ) be rounded down.

# Software testing

At this point, two intact tibia (First subject: female, 45 years old, 161 cm tall; second subject: male, 38 years old, 177 cm tall) were used. Using CT images and image processing, a three-dimensional model was created. Images were taken by bi-directional scanner (model: SIEMON/EMOTION, resolution: 512 × 512 pixels) with a 1.199 mm slice increment. After photographing the bones, a threedimensional model was created by image processing and was cut into two modes in the software. The first cut was parallel to the slope, and for the second, a non-parallel cut was performed. Then, by using the obtained formulas, a gap was created and regulated for both bones to the corrected angle of 10°, and the angles were measured. This section shows the formula in an ideal case.

# Cadaveric study

Five fresh proximal tibia cadavers were prepared. The anteroposterior and true lateral X-ray were tacked, and the tibia slopes were determined in all models. In the working room, Point Twos were first determined in the anteromedial tibial cortex to be 25 mm apart (**Figure 3A** and **3B**).

Two wires were then inserted at determined points from medial to lateral side; they reached each other at Point One on the lateral side (**Figure 4A** and **4B**). This procedure was done under fluoroscopic control using an ACL guide device.

Using the identically-sized pins, the length of the anterior  $(L_1)$  and posterior  $(L_2)$  distances from determined points to the lateral cortex were measured.

Then the proximal tibial cut was made proximal to the tibial tuberosity without considering the tibial slope. It was planned to correct all specimens 10°. Using the table, the anterior and posterior gaps were opened with a scaled spreader, the osteotomy site was fixed with a T buttress plate, and AP and true lateral x-says were taken. The tibial slope and amount of correction were measured on the x-rays (**Figure 5**).

# Results

# Software results of osteotomy tibia

Each bone was tested twice: one with a slope cut parallel, and one with a slope cut non-parallel to the tibial slope. The osteotomy was done proximal to the tibial tuberosity. Two charts for each cut were presented that showed actual modified varus angle and changes in slope angle versus different (expected) varus angles.

The measured parameters calculated by computer for the two subjects are shown in **Table 1**.

# Novel technique in open wedge HTO

**Table 4.** Values of H and S corresponding to the  $L_1$  and  $L_2$ 

									2		L, (r	nm)										
		55	56	57	58	59	60	61	62	63	64	65	66	67	68	69	70	71	72	73	74	75
L <sub>2</sub>	55	53.56																				
(mm)		12.50																				
	56	54.03	54.59																			
		10.28	12.50																			
	57	54.41	55.06	55.61																		
	_	8.02	10.24	12.50																		
	58	54.70	55.43	56.08	56.64																	
		5.72	7.94	10.20	12.50																	
	59	54.90	55.72	56.46	57.10	57.66																
		3.38	5.60	7.86	10.16	12.50																
	60	54.99	55.91	56.74	57.48	58.13	58.68															
		1.00	3.22	5.48	7.78	10.12	12.50															
	61	54.98	55.99	56.92	57.75	58.50	59.15	59.71														
		-1.42	0.80	3.06	5.36	7.70	10.08	12.50														
	62	54.86	55.98	57.00	57.93	58.77	59.51	60.17	60.73													
		-3.88	-1.66	0.60	2.90	5.24	7.62	10.04	12.50													
	63	54.63	55.85	56.97	58.00	58.94	59.78	60.53	61.19	61.75												
		-6.38	-4.16	-1.90	0.40	2.74	5.12	7.54	10.00	12.50												
	64	54.27	55.60	56.83	57.96	59.00	59.94	60.79	61.55	62.21	62.77											
		-8.92	-6.70	-4.44	-2.14	0.20	2.58	5.00	7.46	9.96	12.50											
	65	53.78	55.23	56.57	57.81	58.95	60.00	60.95	61.81	62.57	63.23	63.79										
		-11.50	-9.28	-7.02	-4.72	-2.38	0.00	2.42	4.88	7.38	9.92	12.50										
	66	53.16	54.72	56.18	57.53	58.79	59.94	61.00	61.96	62.82	63.58	64.24	64.81									
		-14.12		-9.64	-7.34	-5.00	-2.62	-0.20	2.26	4.76	7.30	9.88	12.50									
	67	52.38	54.07	55.66	57.13	58.50	59.77	60.93	62.00	62.96	63.83	64.60	65.26	65.82								
			-14.56	-12.30	-10.00	-7.66	-5.28	-2.86	-0.40	2.10	4.64	7.22	9.84	12.50								
	68	51.43	53.27	54.99	56.59	58.08	59.47	60.75	61.92	63.00	63.97	64.84	65.61	66.28	66.84							
		-19.48	-17.26	-15.00	-12.70	-10.36	-7.98	-5.56	-3.10	-0.60	1.94	4.52	7.14	9.80	12.50							
	69	50.31	52.31	54.17	55.91	57.53	59.03	60.43	61.72	62.91	63.99	64.98	65.85	66.63	67.30	67.86						
	70		-20.00	-17.74	-15.44	-13.10	-10.72	-8.30	-5.84	-3.34	-0.80	1.78	4.40	7.06	9.76	12.50	00.07					
	70	48.99	51.16	53.18	55.06	56.82	58.46	59.99	61.40	62.70	63.90	64.99	65.98	66.86	67.64	68.31	68.87					
	74	-25.00	-22.78	-20.52	-18.22	-15.88	-13.50	-11.08	-8.62	-6.12	-3.58	-1.00	1.62	4.28	6.98	9.72	12.50	<u> </u>				
	71	47.45	49.81	52.00	54.05	55.96	57.74	59.40	60.94	62.36	63.68	64.89	65.99	66.98	67.87	68.65	69.33	69.89				
	70	-27.82	-25.60	-23.34	-21.04	-18.70	-16.32	-13.90	-11.44	-8.94	-6.40	-3.82	-1.20	1.46	4.16	6.90	9.68	12.50	70.01			
	12	45.65	48.23	50.62	52.85	54.92	56.85	58.65	60.33	61.89	63.33	64.66	65.88	66.99	67.99	68.88	69.67		70.91			
	72	-30.68	-28.46 46.40	-26.20 49.01	-23.90 51.44	-21.56 53.69	-19.18 55.79	-16.76 57.74	-14.30 59.57	-11.80 61.26	-9.26 62.83	-6.68 64.29	-4.06 65.63	-1.40 66.86	1.30 67.98	4.04 68.99	6.82 69.89	9.64 70.68	12.50 71.36	71.92		
	15		-31.36	-29.10	-26.80	-24.46	-22.08	-19.66	-17.20		-12.16	-9.58	-6.96	-4.30	-1.60					12.50		
	74									-14.70						1.14	3.92	6.74	9.60		72.04	
	/4	41.13 -36.52	44.27	47.14	49.79 -29.74	52.25	54.53 25.02	56.66	58.64 20.14	60.48	62.19 15.10	63.78	65.25	66.61 7.24	67.85 4 5 4	68.98 1 80	69.99	70.90	71.69	72.37	72.94	
	75	-36.52	-34.30 41.79	-32.04 44.97	-	-27.40	-25.02	-22.60	-20.14	-17.64 59.53	-15.10	-12.52	-9.90	-7.24	-4.54	-1.80 68.83	0.98	3.80	6.66	9.56	12.50	72.05
	15				47.89	50.58	53.07	55.38	57.53		61.39	63.12	64.73	66.22	67.58		69.97	71.00	71.91	72.70	73.39	73.95
		-39.50	-37.28	-35.02	-32.72	-30.38	-28.00	-25.58	-23.12	-20.62	-18.08	-15.50	-12.88	-10.22	-7.52	-4.78	-2.00	0.82	3.68	6.58	9.52	12.50

Table 5. Values of A and B corresponding to the and Correction angle  $(\theta)$ 

									Corr	ection	angle (	α) [deg	]									
		35	36	37	38	39	40	41	42	43	44	45	46	47	48	49	50	51	52	53	54	55
Correction angle ( $\alpha$ ) [deg]	1	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.0
		0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.01	0.0
	2	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.0
		0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.02	0.0
	3	0.03	0.03	0.03	0.03	0.03	0.03	0.03	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.
		0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.04	0.03	0.03	0.03	0.03	0.03	0.03	0.
	4	0.04	0.04	0.04	0.04	0.04	0.04	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.06	0.06	0.06	0
		0.06	0.06	0.06	0.06	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.05	0.04	0.04	0.04	0.04	0.04	0
	5	0.05	0.05	0.05	0.05	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.07	0.07	0.07	0.07	0.07	0.07	0.07	0
	_	0.07	0.07	0.07	0.07	0.07	0.07	0.07	0.07	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.06	0.05	0.05	0.05	0
	6	0.06	0.06	0.06	0.06	0.07	0.07	0.07	0.07	0.07	0.07	0.07	0.08	0.08	0.08	0.08	0.08	0.08	0.08	0.08	0.09	0.
		0.09	0.09	0.08	0.08	0.08	0.08	0.08	0.08	0.08	0.08	0.07	0.07	0.07	0.07	0.07	0.07	0.07	0.06	0.06	0.06	0.
	7	0.07	0.07	0.07	0.08	0.08	0.08	0.08	0.08	0.08	0.09	0.09	0.09	0.09	0.09	0.09	0.09	0.10	0.10	0.10	0.10	0
	_	0.10	0.10	0.10	0.10	0.10	0.09	0.09	0.09	0.09	0.09	0.09	0.09	0.08	0.08	0.08	0.08	0.08	0.08	0.07	0.07	0
	8	0.08	0.08	0.08	0.09	0.09	0.09	0.09	0.09	0.10	0.10	0.10	0.10	0.10	0.10	0.11	0.11	0.11	0.11	0.11	0.11	0
		0.12	0.11	0.11	0.11	0.11	0.11	0.11	0.10	0.10	0.10	0.10	0.10	0.10	0.09	0.09	0.09	0.09	0.09	0.08	0.08	0
	9	0.09	0.09	0.10	0.10	0.10	0.10	0.10	0.11	0.11	0.11	0.11	0.11	0.12	0.12	0.12	0.12	0.12	0.12	0.13	0.13	0
	_	0.13	0.13	0.13	0.12	0.12	0.12	0.12	0.12	0.12	0.11	0.11	0.11	0.11	0.11	0.10	0.10	0.10	0.10	0.10	0.09	0
	10	0.10	0.10	0.11	0.11	0.11	0.11	0.12	0.12	0.12	0.12	0.12	0.13	0.13	0.13	0.13	0.14	0.14	0.14	0.14	0.14	0
		0.14	0.14	0.14	0.14	0.14	0.14	0.13	0.13	0.13	0.13	0.12	0.12	0.12	0.12	0.12	0.11	0.11	0.11	0.11	0.10	0
	11		0.11	0.12	0.12	0.12	0.12	0.13	0.13	0.13	0.14	0.14	0.14	0.14	0.14	0.15	0.15	0.15	0.15	0.16	0.16	0
		0.16	0.16	0.16	0.15	0.15	0.15	0.15	0.14	0.14	0.14	0.14	0.14	0.13	0.13	0.13	0.12	0.12	0.12	0.12	0.11	0
	12	0.12	0.12	0.13	0.13	0.13	0.14	0.14	0.14	0.14	0.15	0.15	0.15	0.16	0.16	0.16	0.16	0.17	0.17	0.17	0.17	0
		0.17	0.17	0.17	0.17	0.17	0.16	0.16	0.16	0.16	0.15	0.15	0.15	0.14	0.14	0.14	0.14	0.13	0.13	0.13	0.12	0
	13	0.13	0.14	0.14	0.14	0.15	0.15	0.15	0.15	0.16	0.16	0.16	0.17	0.17	0.17	0.17	0.18	0.18	0.18	0.18	0.19	0
		0.19	0.19	0.18	0.18	0.18	0.18	0.17	0.17	0.17	0.17	0.16	0.16	0.16	0.15	0.15	0.15	0.15	0.14	0.14	0.14	0
	14	0.14	0.15	0.15	0.15	0.16	0.16	0.16	0.17	0.17	0.17	0.18	0.18	0.18	0.19	0.19	0.19	0.19	0.20	0.20	0.20	0
		0.20	0.20	0.20	0.20	0.19	0.19	0.19	0.19	0.18	0.18	0.18	0.17	0.17	0.17	0.16	0.16	0.16	0.15	0.15	0.15	0
	15	0.15	0.16	0.16	0.16	0.17	0.17	0.18	0.18	0.18	0.19	0.19	0.19	0.20	0.20	0.20	0.21	0.21	0.21	0.21	0.22	0
		0.22	0.22	0.21	0.21	0.21	0.21	0.20	0.20	0.20	0.19	0.19	0.19	0.18	0.18	0.18	0.17	0.17	0.16	0.16	0.16	0
	16		0.17	0.17	0.18	0.18	0.18	0.19	0.19	0.20	0.20	0.20	0.21	0.21	0.21	0.22	0.22	0.22	0.23	0.23	0.23	0.
		0.23	0.23	0.23	0.23	0.22	0.22	0.22	0.21	0.21	0.21	0.20	0.20	0.20	0.19	0.19	0.18	0.18	0.18	0.17	0.17	0
	17	0.18	0.18	0.18	0.19	0.19	0.20	0.20	0.20	0.21	0.21	0.22	0.22	0.22	0.23	0.23	0.23	0.24	0.24	0.24	0.25	0.
		0.25	0.25	0.24	0.24	0.24	0.23	0.23	0.23	0.22	0.22	0.22	0.21	0.21	0.20	0.20	0.20	0.19	0.19	0.18	0.18	0
	18	0.19	0.19	0.20	0.20	0.20	0.21	0.21	0.22	0.22	0.23	0.23	0.23	0.24	0.24	0.25	0.25	0.25	0.26	0.26	0.26	0.
		0.27	0.26	0.26	0.26	0.25	0.25	0.25	0.24	0.24	0.23	0.23	0.23	0.22	0.22	0.21	0.21	0.20	0.20	0.20	0.19	0.
	19	0.20	0.20	0.21	0.21	0.22	0.22	0.23	0.23	0.23	0.24	0.24	0.25	0.25	0.26	0.26	0.26	0.27	0.27	0.27	0.28	0.
		0.28	0.28	0.27	0.27	0.27	0.26	0.26	0.26	0.25	0.25	0.24	0.24	0.23	0.23	0.23	0.22	0.22	0.21	0.21	0.20	0.
	20	0.21	0.21	0.22	0.22	0.23	0.23	0.24	0.24	0.25	0.25	0.26	0.26	0.27	0.27	0.27	0.28	0.28	0.29	0.29	0.29	0.
		0.30	0.29	0.29	0.29	0.28	0.28	0.27	0.27	0.27	0.26	0.26	0.25	0.25	0.24	0.24	0.23	0.23	0.22	0.22	0.21	0.

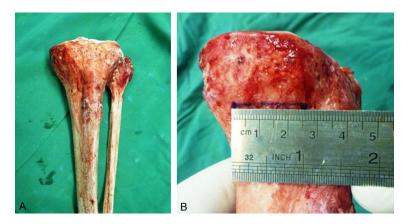


Figure 3. A and B: Determining two points (2.5 cm apart) on anteromedial cortex.

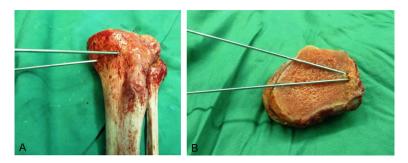


Figure 4. (A and B) Inserting two pins from determined points (A) to cross on lateral cortex (B).

In **Figure 6**, the varus angles calculated by different methods depending on the modified varus angle (expected) were plotted from zero to 20°. The gray curve showed the exact solution of the nonlinear numerical solution of the 7 equations system, and the 7 unknowns were obtained. The black curve was solved using a simple formula by which the error was less than 0.2°. The blue and red point-line curves showed the performance when using tables for non-parallel (slope increase of 5° for the first subject and 10° for the second) and parallel cutting. As shown, the error was less than 0.5° when using the table.

In comparing curves A with B in **Figure 6**, no significant difference was seen between the figures. This result showed the efficiency of this method in response to different conditions. In order to achieve modified varus angle correction, **Tables 4** and **5** or the formulas could be used.

In **Figure 7**, the changes in slope angle using the simplified formulas and tables were pre-

sented. It was clear that the results of seven simultaneous exact equations were always zero. In the curve that was related to the simplified formula, (black continuous curve), an increase in the slope angle in respect to the increase in the angle of the varus correction was seen. This increase was less than 0.5° in both subjects. In the curve related to use of the tables, slope angles increased in all cases but one, and all were less than 1.

In **Table 3**, a comparison of changes in slope using the two mentioned ways were presented. Based on the *p*-value, the simplified formula or the tables could be used to correct the varus, or least change in the slope without osteotomy angle.

From the low *p*-value it could be concluded that assuming a value of less than 1 is not a fail, and we could calculate

that the median of the data was less than 1 in this domain Table 2.

Results from osteotomies on 5 bones were presented in **Table 3**. In this experiment, subject 2's bone was broken in the procedure and was therefore eliminated. To compress the data, the value of the varus correction for all subjects was assumed to be 10°. As seen in **Table 3**, the changes in the angle of the slopes were significantly small. In 3 subjects, the change was less than 0.6°. Especially in subjects 3 and 4, the correction of the varus was significantly close to 10° (the desired value) **Figure 8**.

# Discussion

The successful correction of misalignment by a medial opening wedge osteotomy has been reported [8-11]. A number of technical improvements have contributed to the safety and reproducibility of this technique [12]. Advantages of this technique include the requirement for only a single osteotomy with surgical dissection away from the peroneal nerve, no violation of the fibula and tibiofibular joint, and the capabil-

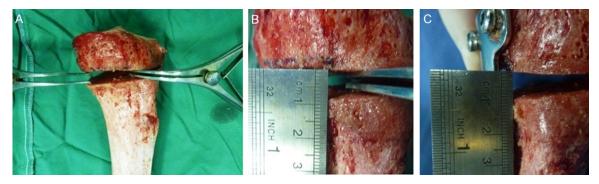
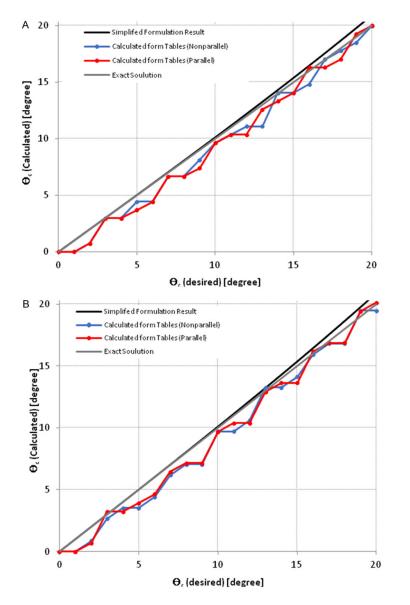


Figure 5. A-C: Opening anterior and posterior gaps and fixation.



**Figure 6.** Comparative diagrams of different methods for varus modified angle correction from zero to 20 degrees. (A and B are related to first and second subject respectively).

ity for intrao perative adjustment of the correction. Other advantages of opening wedge osteotomy may include a more precise correction, enhancement of bone stock, the avoidance of changes in the proximal morphologic characteristics of the tibia, and the possibility of correcting large deformities. Additionally, some surgeons believe that concomitant ACL reconstruction may be easier with the medial opening wedge approach. Inherent disadvantages include the potential need to procure an autogenous bone graft and the use of an alternative bone graft source such as an allograft or a synthetic bone graft substitute [8]. New fixation devices, such as the Puddhu plate [13] and the TomoFix [13, 14], have been specifically developed for medial opening wedge osteotomies.

Although HTOs were initially performed to correct deformities in the coronal plane, opening wedge osteotomies can simultaneously alter tibial slope in the sagittal plane [5, 15, 16].

Street et al. showed that medial opening wedge osteotomy inadvertently changes posterior tibial slope. In their study on 82 knees with varus arthrosis, they found that medial opening wedge osteotomy may alter the

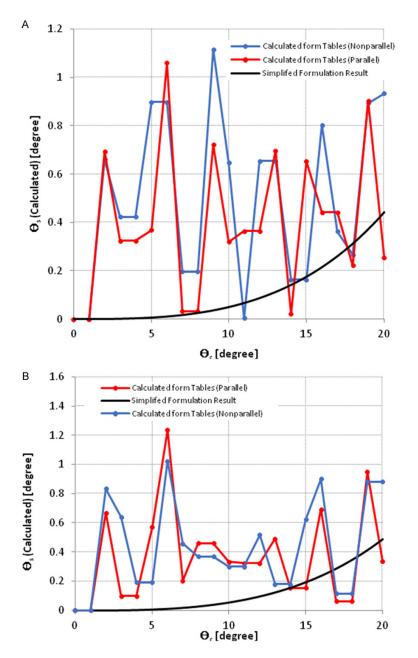


Figure 7. The comparative diagrams of changing varus angle with respect to changes of varus modified angle from zero to 20. (A and B are related to first and second subject respectively).

sagittal alignment by increasing the posterior tibial slope [17].

Many studies have been done to keep the slope unchanged in medial open wedge osteotomy, but they are not practical [18].

Song et al., in their study on forty cases of navigation-assisted open-wedge HTO, showed that in virtual surgery, a ratio of 0.67 between the anterior and posterior gap was needed to maintain the original slope [18].

In their study on proximal tibial open wedge osteotomy using triangular CT scan, Noyes et al. showed that, in order to keep the tibial slope unchanged, as a rule of thumb, the diameter of the anterior gap at the osteotomy site must be half that of the posterior gap on the posteromedial side; however, using this method, the tibial slope will change up to 1-2° [7].

All these rules are based on the assumption that, during surgery, the osteotomy line is parallel to the proximal tibial plateau [19].

Performing the osteotomy parallel to the proximal tibial plateau is an important step in the osteotomy method [19]. but it is sometimes difficult to find the tibial plateau during the osteotomy. In the current study, a new osteotomy technique was considered in which a proximal tibial osteotomy was performed regardless of the proximal tibial plateau. Based on the mathematical formula, a table was introduced to facilitate the technique. Based on this study, the surgeon can measure the lengths of L<sub>1</sub> and L<sub>2</sub> intraoperatively, and using the table's data, the desired amount of correction can be achieved

with less than  $1.4^{\circ}$ . The most important advantages of the method of the current study are that it does not need to consider the osteotomy line parallel to the tibial plateau and changes in the slope are minimal (mean = 0.6).

There were some limitations in this study, the first is the amount of correction desired. An amount of  $10^{\circ}$  is considered in all models. Although the technique is applicable for all

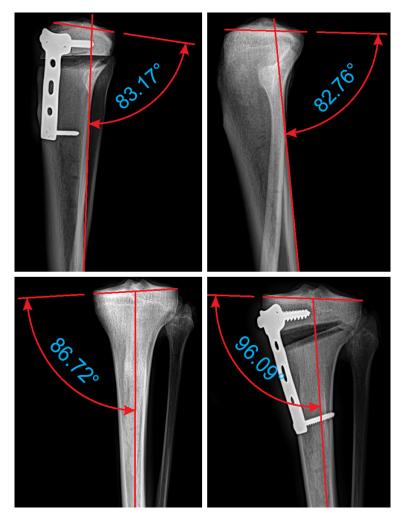


Figure 8. Change in slope angle after osteotomy (10 degree correction) in the fourth cadaveric subject.

desired degrees of correction, further cadaveric studies are needed to evaluate the technique for different varus angles.

Another limitation was the level of technical difficulty. In this method, two guide wires in the proximal tibia should reach in one point in the lateral cortex which may be challenging to the surgeon. The use of fluoroscopy and ACL guides to facilitate pin insertion is recommended, but easier methods should be investigated. A useful and fully mechanical device is invented for this aim (named OsteoGuide) by this team.

In conclusion, use of this new technique in open wedge HTO can result in good varus correction with minimal changes to the tibial slope, regardless of the orientation of the osteotomy line.

# Acknowledgements

The authors would like to thank head of imam Khomeini hospital tissue bank organization for their great collaboration in preparing fresh cadaver for this article without their help this work could not be completed.

#### Disclosure of conflict of interest

None.

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